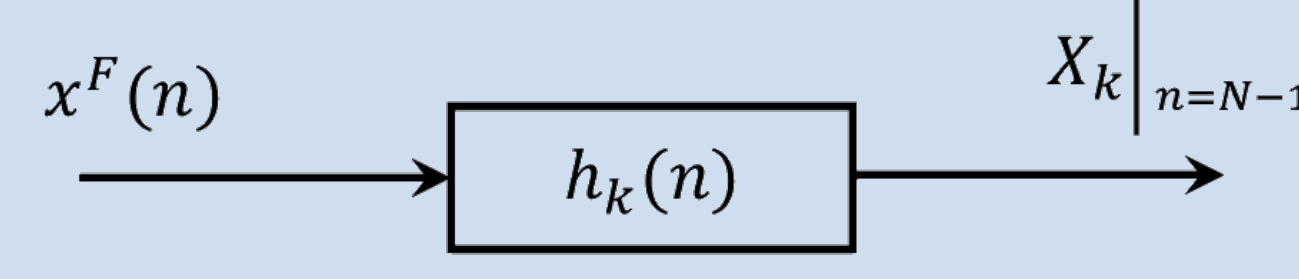
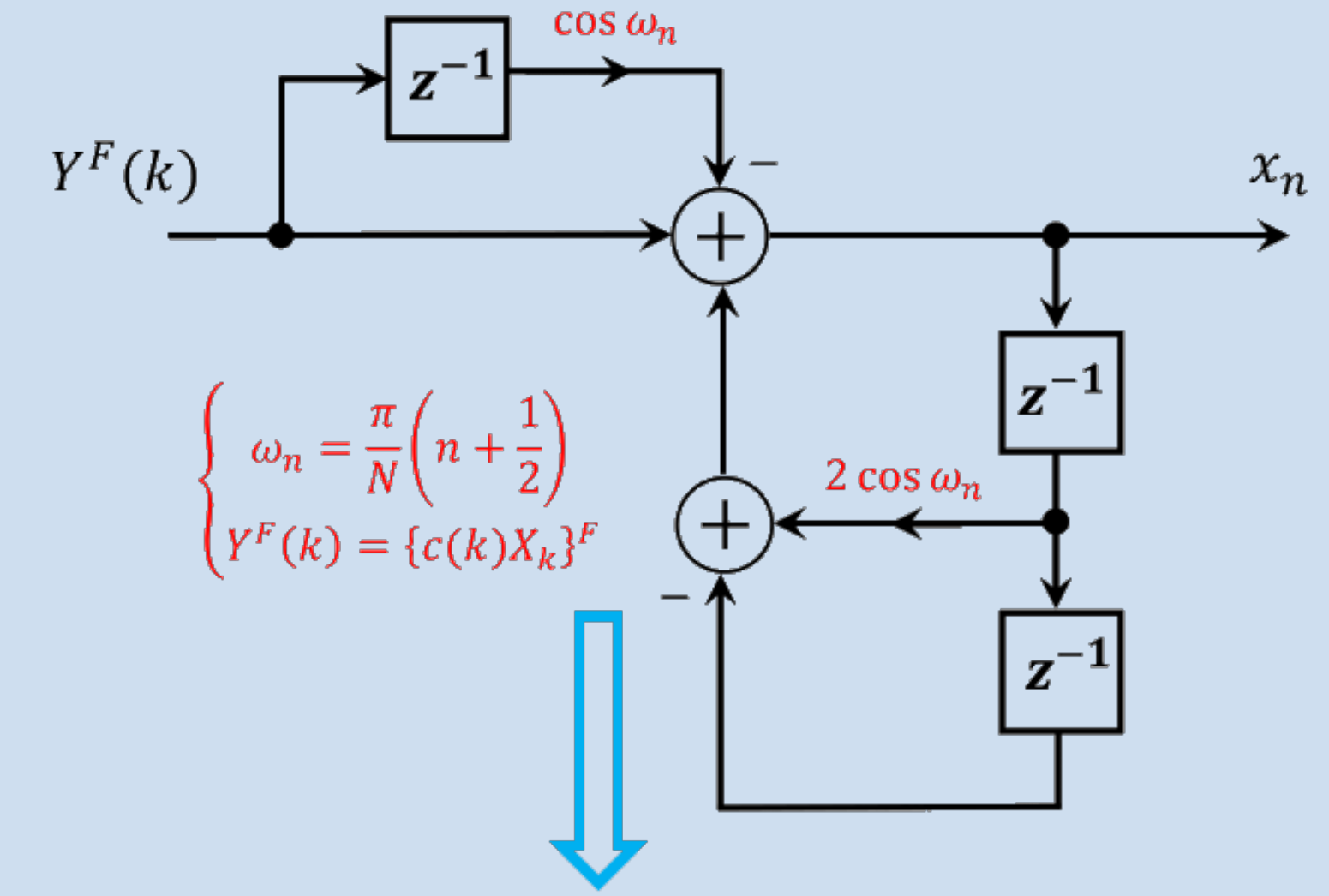
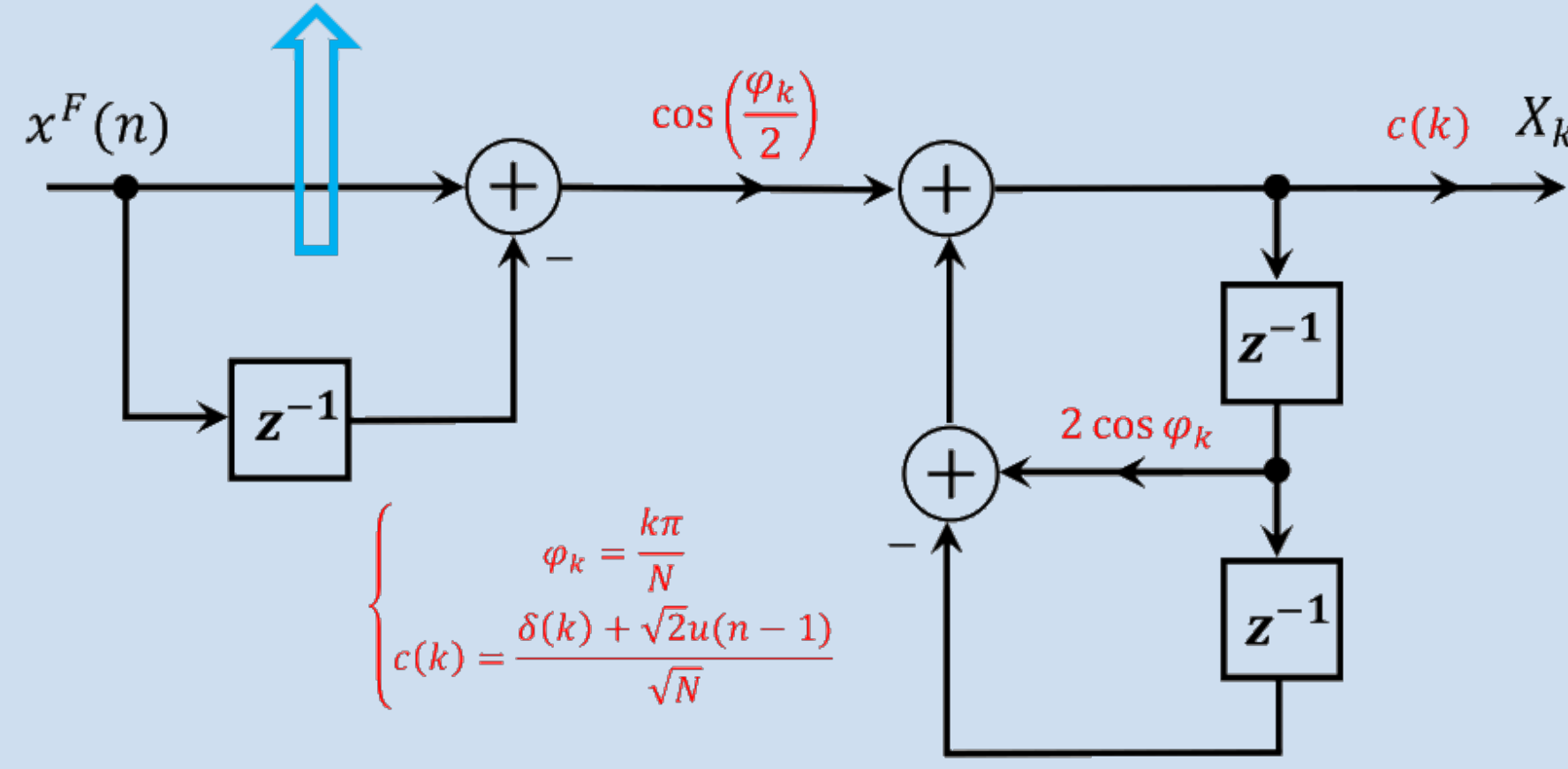


## DCT/IDCT Filter Formulation

- Theorem:** A discrete transformation of a discrete signal,  $f(n)$  of length  $N$ , over a kernel function of  $g(n, k)$  can be derived by the discrete convolution of the kernel and the flipped signal which is evaluated at  $N - 1$ .



- $X_k = c(k) \sum_{n=0}^{N-1} x(n) \cos \left[ \frac{\pi}{N} \left( n + \frac{1}{2} \right) k \right] = c(k) \left\{ x^F(n) * h_k(n) \right\}_{n=N-1} \Rightarrow H_k(z) = \frac{\alpha_k (1 - z^{-1})}{1 - 2z^{-1} \cos \varphi_k + z^{-2}}$  where  $\alpha_k = \cos \left( \frac{\varphi_k}{2} \right)$ .

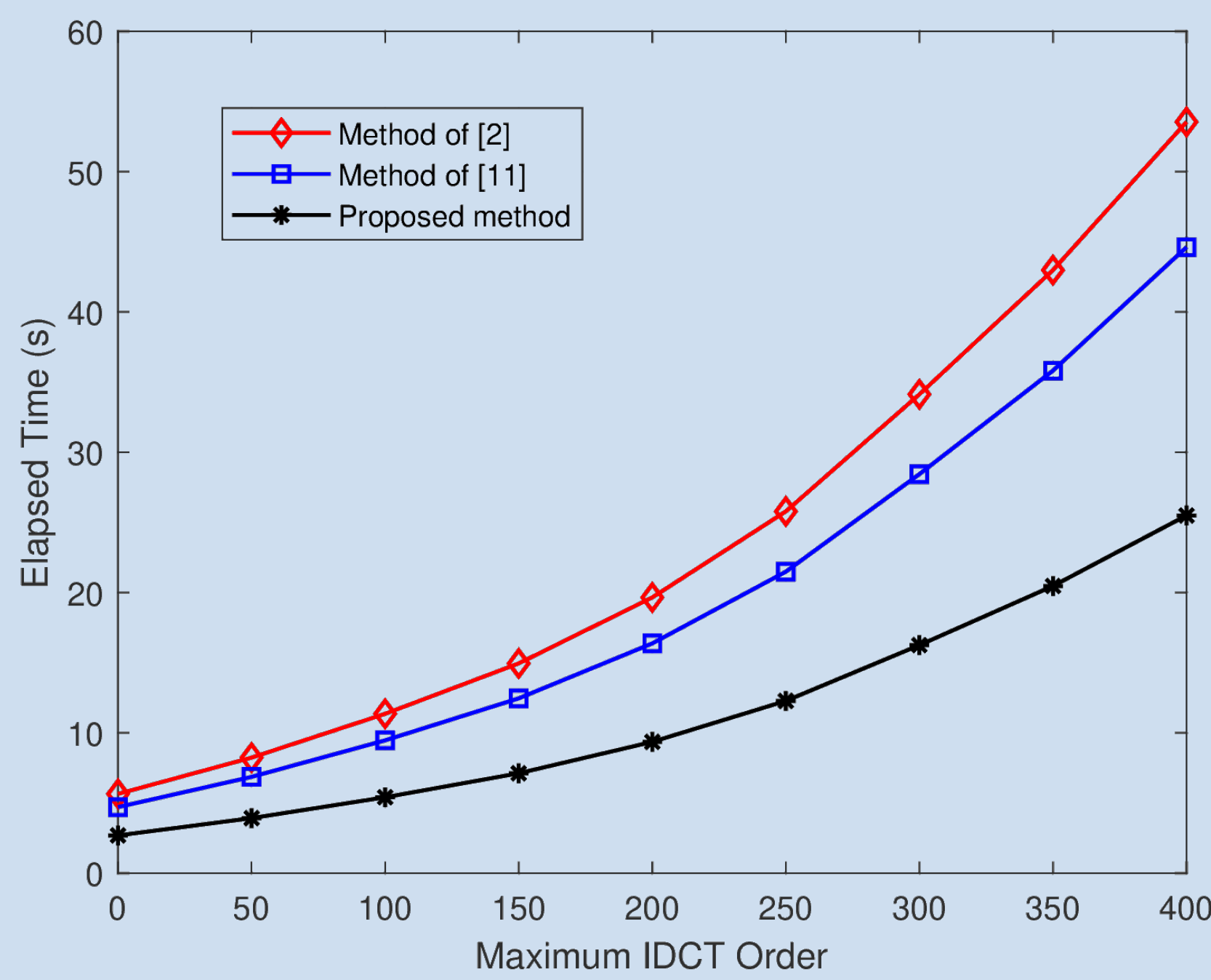
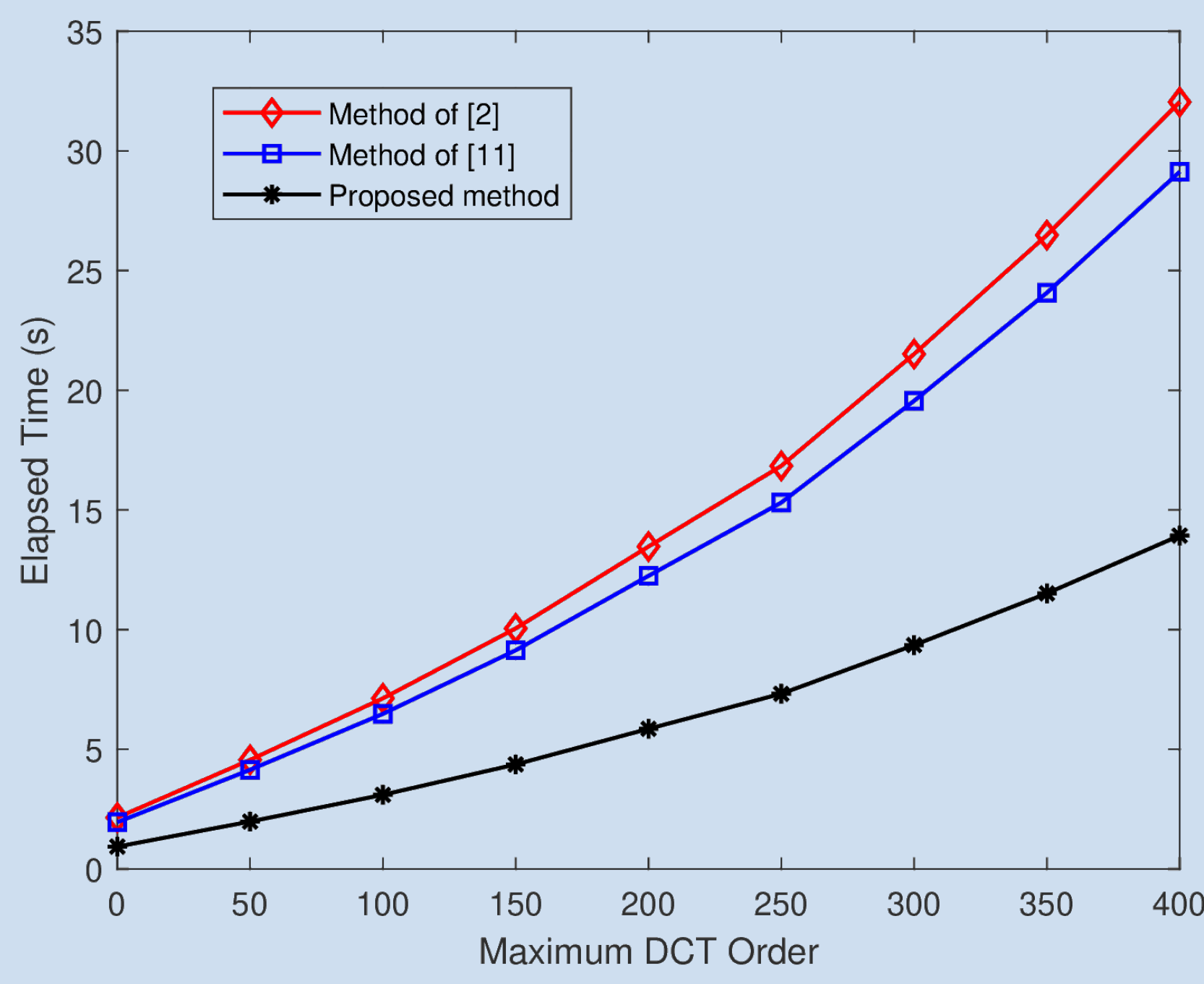


- $x(n) = \sum_{k=0}^{N-1} c(k)X_k \cos \left[ \frac{\pi}{N} \left( n + \frac{1}{2} \right) k \right] = Y^F(k) * h_n(k) \Big|_{k=N-1} \Rightarrow H_n(z) = \frac{1 - z^{-1} \cos \omega_n}{1 - 2z^{-1} \cos \omega_n + z^{-2}}$  where  $\omega_n = \frac{\pi}{N} \left( n + \frac{1}{2} \right)$ .

## Computational Time

Number of multiplication and addition operations for computation of DCT coefficients based on three different methods for all fetus ultrasound test images with size  $400 \times 400$ .

Operation	Fast algorithms		Proposed algorithm
	[2]	[11]	
Multiplication	560	245	<b>162</b>
Addition	2450	N/A	<b>520</b>



## Acknowledgements & Ref.

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[2] Che-Hong Chen *et al.*, IEEE Transactions on Circuits and Systems I: Regular Papers, vol. 51, no. 10, pp. 2017–2030, Oct 2004.

[11] S. Tsai and S.-M. Yang, Mathematical Problems in Engineering, vol. 2017, 2017.

## Experiments

- DCT-Wiener filtering

$$\hat{\mathbf{H}}_{\mathbf{W}}(\mathbf{k}_1, \mathbf{k}_2) = \frac{\hat{\mathbf{P}}_{\mathbf{x}}(\mathbf{k}_1, \mathbf{k}_2)}{\hat{\mathbf{P}}_{\mathbf{x}}(\mathbf{k}_1, \mathbf{k}_2) + \lambda(\mathbf{k}_1, \mathbf{k}_2)\sigma^2}$$

$\hat{H}_W(k_1, k_2)$  is an estimate of the frequency re-

sponse of the Wiener filter,  $\hat{P}_x(k_1, k_2)$  is power spectral density estimates of the noise-free image and  $\sigma^2$  is noise variance since  $\lambda(k_1, k_2)$  is proportional to the image size.

- DCT Filtering results for the real fetal ultrasound images

	Original image	DCT-based denoised image (proposed method)			Wiener filter denoised image
Normal Fetus					
	Threshold level ( $\beta$ )	0.8	0.5	0.1	N/A
	SNIRE	20.6797	17.0367	<b>6.7440</b>	<b>10.1939</b>
	BRISQUE	53.0698	50.2022	<b>45.4849</b>	<b>48.667</b>
Fetal Cystic Hydruma					
	Threshold level ( $\beta$ )	0.8	0.5	0.1	N/A
	SNIRE	19.8847	16.6770	<b>6.6088</b>	<b>9.4221</b>
	BRISQUE	59.2062	58.5306	<b>44.5435</b>	<b>49.2863</b>
Fetal Hydronephrosis					
	Threshold level ( $\beta$ )	0.8	0.5	0.1	N/A
	SNIRE	19.2214	15.2223	<b>6.3865</b>	<b>8.5244</b>
	BRISQUE	59.6799	53.8941	<b>49.1410</b>	<b>56.6273</b>

- Error, similarity and quality metrics:**

- SNIRE** is the Statistical-Normalization Image Reconstruction Error

- BRISQUE** is Blind/Referenceless Image Spatial Quality Evaluator

- SSIM** is the Structural Similarity Index Measure

- Image reconstruction of ultrasound fetus images

	Original image	Reconstructed images based on the proposed IDCT filter				
Normal Fetus						
	Max. Order	50	100	200	300	400
	SNIRE	17.2746	11.4128	6.43499	3.97367	0.765523
	SSIM	0.967772	0.986241	0.995663	0.998343	0.999935
Fetal Cystic Hydruma						
	Max. Order	50	100	200	300	400
	SNIRE	15.5357	11.0797	6.6417	4.16901	1.19042
	SSIM	0.980865	0.990384	0.996564	0.998643	0.999883
Fetal Hydronephrosis						
	Max. Order	50	100	200	300	400
	SNIRE	12.2475	5.42537	2.4452	1.43111	0.394929
	SSIM	0.983393	0.996762	0.999324	0.999761	0.999988

