



A Bayesian Deep CNN Framework for Reconstructing k-t Under-sampled Resting-fMRI

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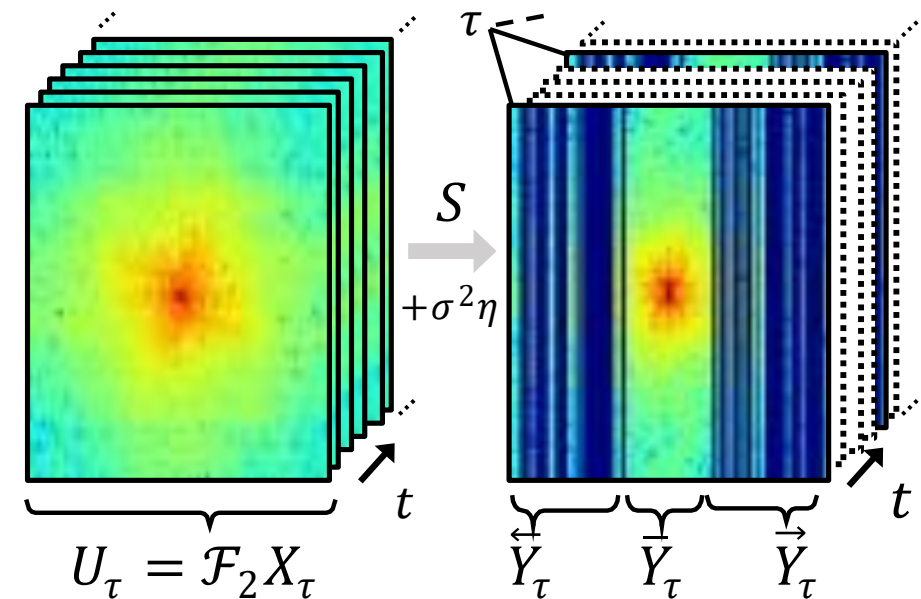
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Introduction

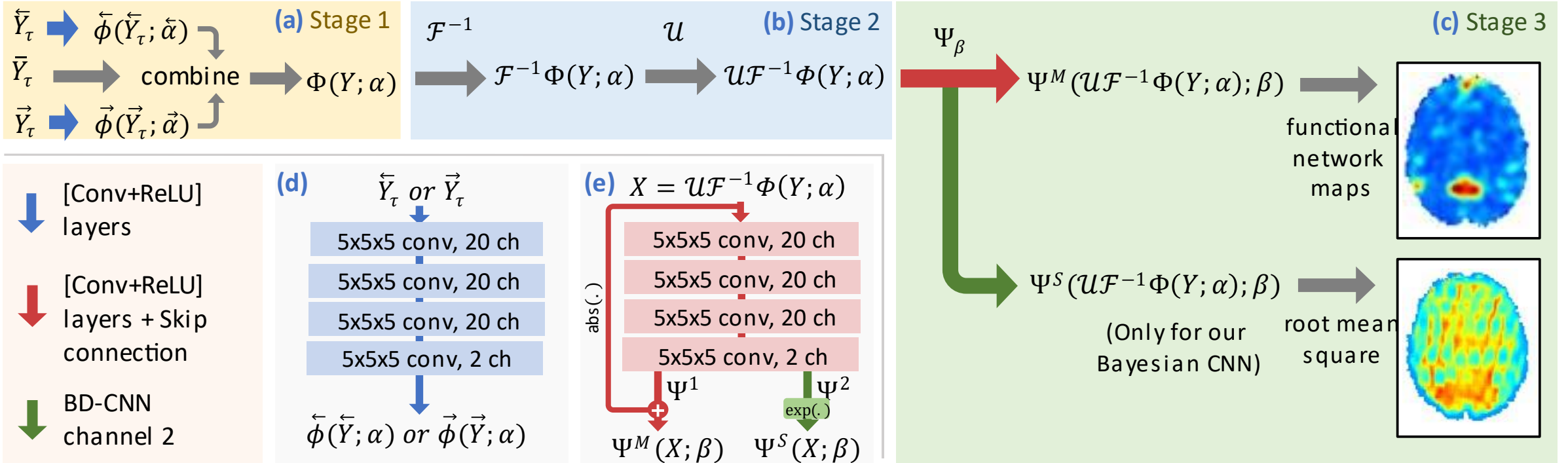
- Under-sampled reconstruction in resting-state fMRI holds the potential to **enable higher spatial resolution** in brain R-fMRI **without increasing scan duration**.
- We propose a novel **convolutional neural network (CNN) framework** to reconstruct R-fMRI from k-t under-sampled data.
- The CNN framework for reconstruction comprises of two jointly-learned multilayer CNN components for
 - i. explicitly **filling in missing k-space data**, using acquired data in frequency-temporal neighborhoods, and
 - ii. image **quality enhancement** in the spatiotemporal domain.
- Results show improvements over all previously know methods, in the connectivity maps for three cerebral functional networks.

Overview

- Subsampling scheme **subsamples both in time and k-space**; and acquisition noise is also added.
- The CNN architecture, with end-to-end learning, has stage
 1. that uses a CNN to fill in missing k-space data using acquired data in k-t-neighborhoods,
 2. that includes a Fourier inverse to transform the data to the spatial domain, and
 3. that uses a CNN learned for image quality enhancement in the spatiotemporal domain.



Model



Loss Functions

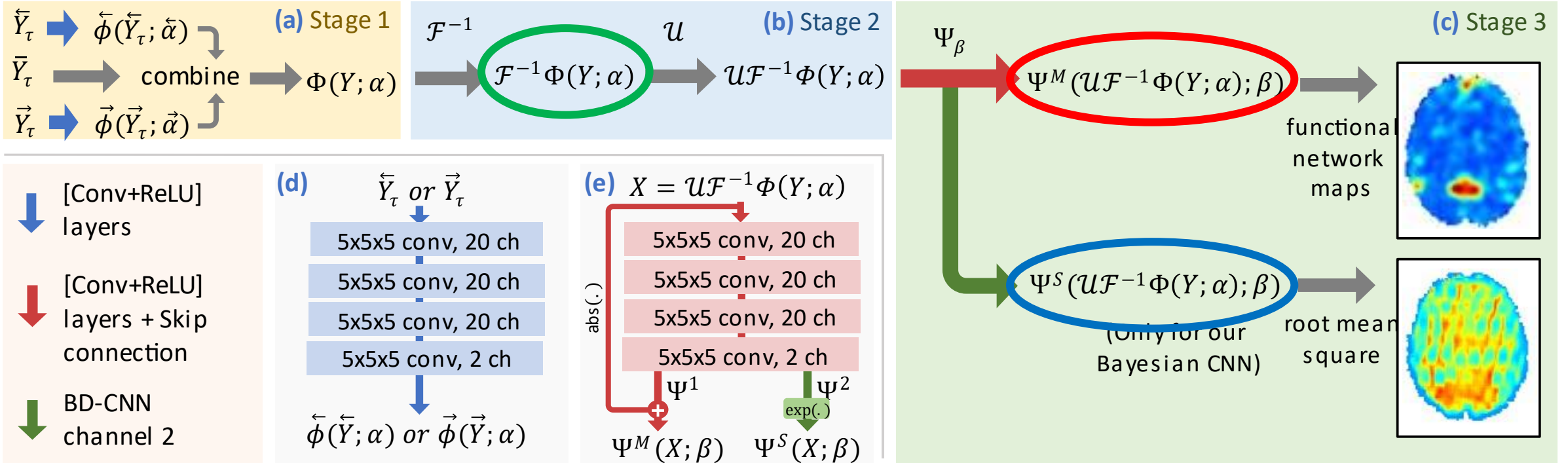
- Mean Squared Loss ($p = 2$)
- Robust Loss ($p = 0.5$)

$$\arg \min_{\alpha, \beta} (1 - \lambda) \sum_n \|X^n - \Psi^M(Y^n; \alpha, \beta)\|_2^p + \lambda \sum_n \sum_\tau \|X_\tau^n - \mathcal{F}^{-1}\Phi(Y_\tau^n; \alpha)\|_2^p$$

- Bayesian Loss

$$\arg \min_{\alpha, \beta} \sum_n \sum_v \sum_t \frac{(X_{vt}^n - \Psi_{vt}^M(Y^n; \alpha, \beta))^2}{\Psi_{vt}^S(Y^n; \alpha, \beta)^2} + 2 \log(\Psi^S(Y^n; \alpha, \beta))$$

Model



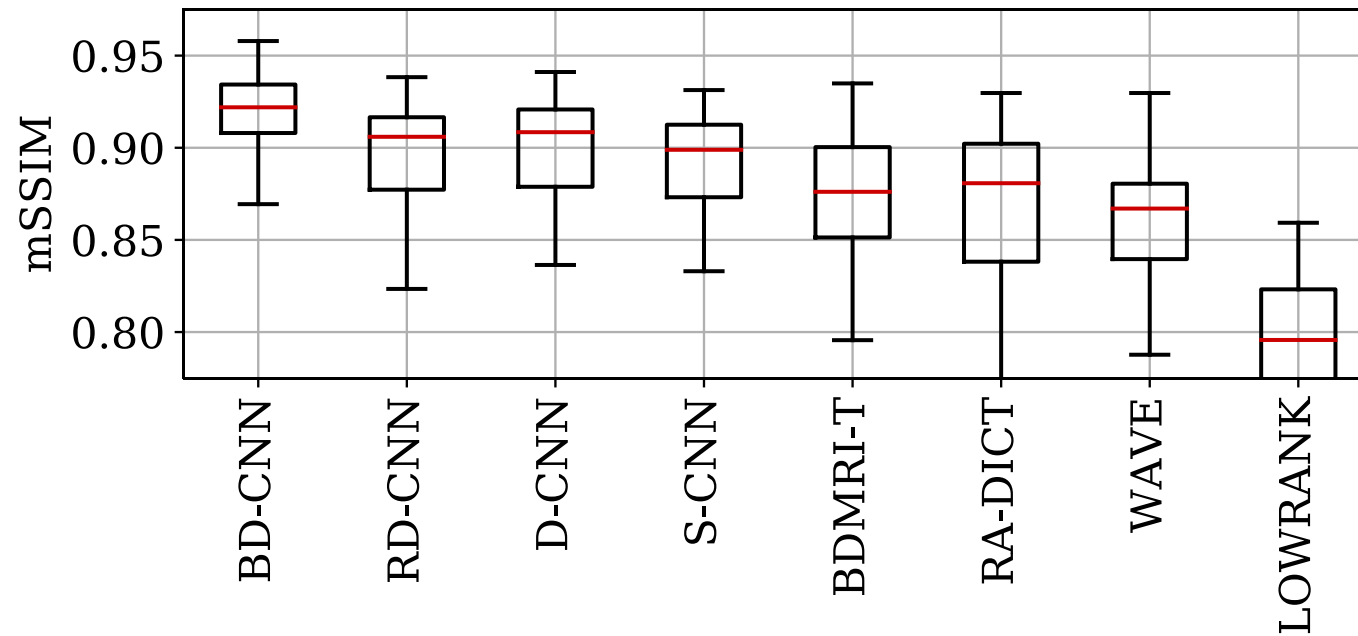
Model Variations

Model	Layers (Φ & Ψ)	Loss
S-CNN	2	Mean squared
D-CNN	4	Mean squared
RD-CNN	4	Robust
BD-CNN	4	Bayesian

Baselines

Model	Description
RA-DICT	A robust data-adaptive sparse dictionary model
WAVE	A sparse wavelet model on the spatiotemporal fMRI signal
LOWRANK	Low-rank model on the joint k-space and temporal domain
BDMRI-T	Adaption of a CNN-based dynamic-MRI reconstruction method

Results on R-fMRI Data from Human Connectome Project



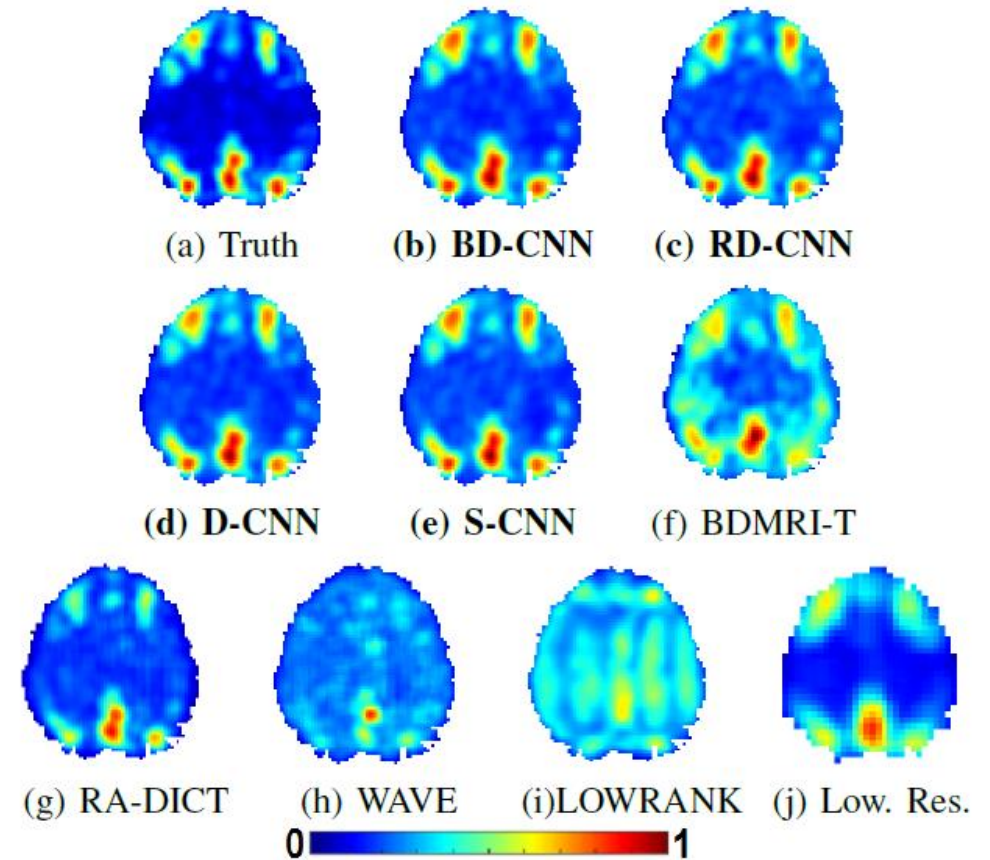
Quantitative Results on Brain R-fMRI. Comparison of all methods, through **mSSIM boxplots** over 50 evaluation-set subjects and all functional-networks.

Results on R-fMRI Data from Human Connectome Project

Qualitative Results on Brain R-fMRI

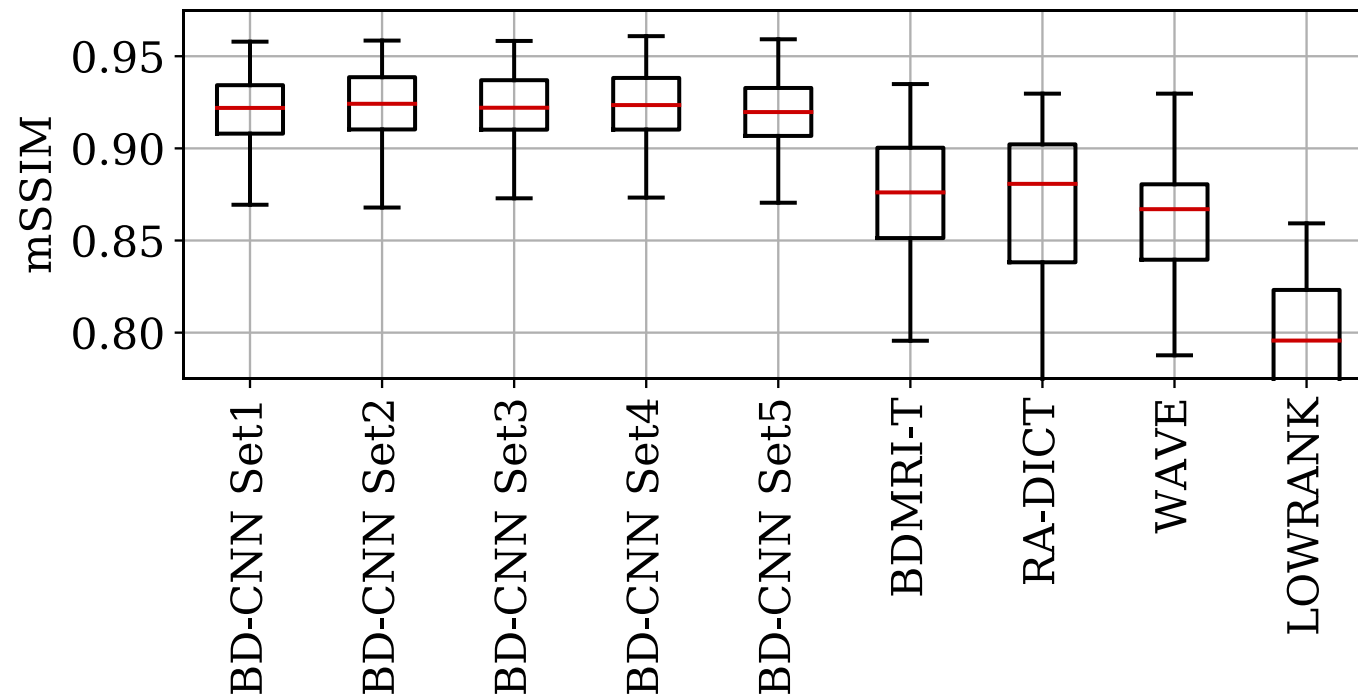
Dorsal Attentive Network (DAN) estimated from

- (a) original data; from fitted models using
- (b) **BD-CNN**: mSSIM 0.93,
- (c) **RD-CNN**: mSSIM 0.92,
- (d) **D-CNN**: mSSIM 0.93,
- (e) **S-CNN**: mSSIM 0.92,
- (f) **BDMRI-T**: mSSIM 0:85,
- (g) **RA-DICT**: mSSIM 0:91,
- (h) **WAVE**: mSSIM 0:85,
- (i) **LOWRANK**: mSSIM 0:74; and from
- (j) 8× lower spatial resolution of (a): mSSIM 0:82.



Inensitivity to Choice of Training and Validation Sets

mSSIM Boxplots over 50 evaluation set subjects and all functional networks, for BD-CNN learned from 5 different training and validation sets.



Performance for Different Values of Free-Parameter λ

Recall:
$$\arg \min_{\alpha, \beta} (1 - \lambda) \sum_n \|X^n - \Psi^M(Y^n; \alpha, \beta)\|_2^p + \lambda \sum_n \sum_\tau \|X_\tau^n - \mathcal{F}^{-1}\Phi(Y_\tau^n; \alpha)\|_2^p$$

- Trend: Performance deteriorates significantly as $\lambda \rightarrow 1^-$.
- Average mSSIM (and standard deviation for all functional networks and evaluation subjects) for $\lambda \in [0, 0.75]$ is 0.90 (0.03), and for $\lambda = 1$ is 0.88 (0.03); demonstrates utility of third stage of our architecture.
- We set $\lambda = 0.5$ because it leads to reduced training time in practice.

Effect of Head Motion

- We simulate head motion for each subject during the 15-minute scan that rotates the head about the spine every minute.
- We choose the rotation angle to generate realistic head motion, and add noise.
- The average mSSIM (and standard deviation) over all functional networks and evaluation subjects are
 - **BD-CNN**: 0.90 (0.04),
 - **BDMRI-T**: 0.87 (0.05),
 - **RA-DICT**: 0.86 (0.06)
 - **WAVE**: 0.86 (0.02),
 - **LOWRANK**: are 0.79 (0.04).

Uncertainty Maps of Reconstruction in Cerebral BOLD Signals

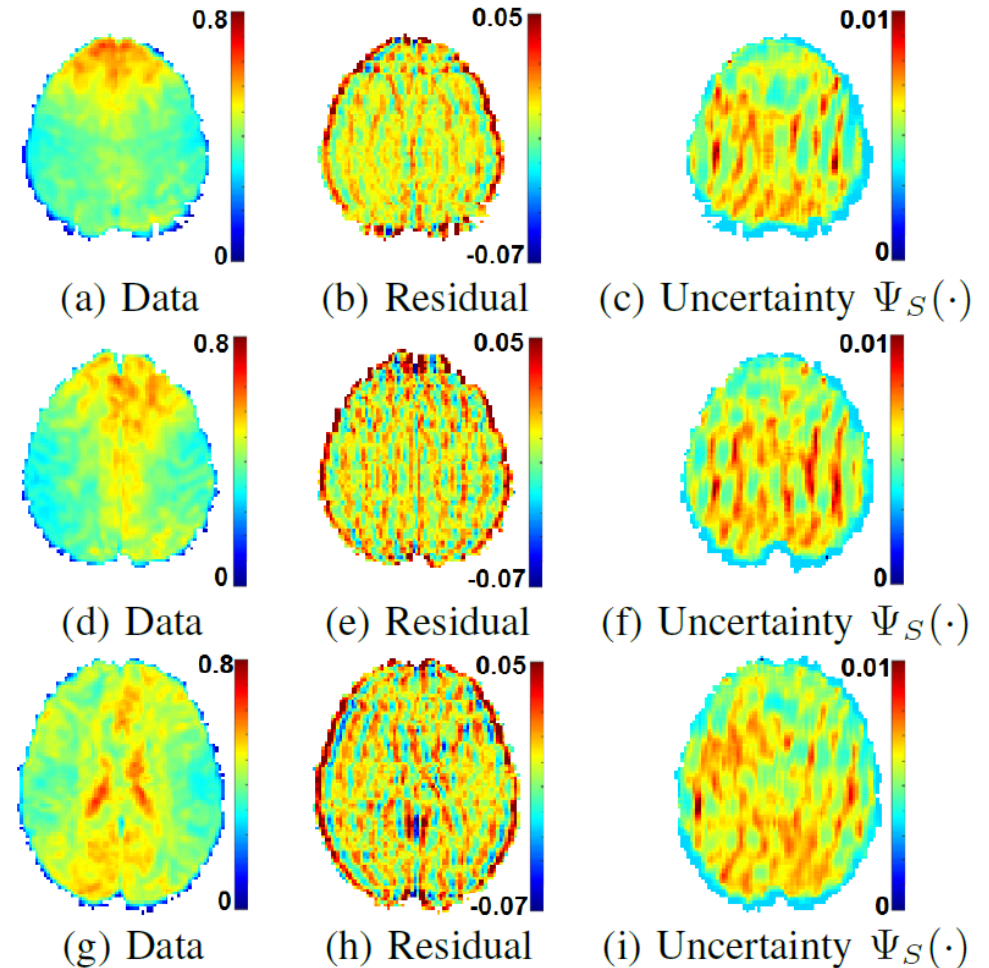
- We can treat the BD-CNN output standard-deviation values as **estimates of the uncertainty**, between voxels, in the reconstructed intensities.
- The artifacts introduced due to k-space under-sampling of the original data are clearly seen in the residuals.
- The corresponding per-voxel standard-deviation maps show higher values (i.e. higher uncertainty) with spatial patterns a similar to those in residuals.

Uncertainty Maps of Reconstruction in Cerebral BOLD Signals

Column 1 (a, d, g) original data,
Column 2 (b, e, h) residual between original data and zero-filled reconstruction, and

Column 3 (c, f, i) per-voxel uncertainty map (standard-deviation map $\Phi^S(\cdot)$) for

- DAN region (row 1),
- ECN region (row 2) and
- DMN region (Row 3).





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Presentation and recording by
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